

# MYOCARDIAL INFARCT DETECTING, SIZING AND LOCATING

## Cross Reference to Related Application

This application claims priority to U.S. Provisional Patent Application Serial No. 60/248,252 filed November 13, 2000 titled "Myocardial Infarct Detecting, Sizing and  
5 Locating", and is hereby incorporated by reference.

## Background and Summary of the Invention

This invention involves conducting an analysis of input ECG and related personal data for the purpose of detecting and giving certain information about sizing and location of old myocardial infarcts (MI). In particular, the invention focuses attention on the general architecture and organization of certain algorithms which play roles in the detection, sizing and locating tasks. Featured among other things as unique in the algorithms architecture of this invention are analyses based upon selected ratios of Q, R and S voltage amplitude values which are associated with ECG data received from certain ECG leads. Two different ECG lead protocols are described herein including the  
15 usual, standard 12-lead protocol, and a known, but less widely employed 15-lead protocol.

In the setting of an interpretation and analysis system employing the algorithms of this invention, input ECG, and certain related personal data, are conventionally collected and fed into the system. This input data can generally be described as follows in relation  
20 to one preferred embodiment and method of practicing the invention, ECG data relating to a particular subject is derived from a conventional 12-lead ECG intake protocol, with data particularly focused upon which comes from leads I, II, V1, V2, V3, V4, V5 and V6.

In a modified form and implementation of the invention, data from a larger, 15-lead input protocol is used, with such data including information from each of the eight specific leads just mentioned above, and in addition, from leads V8R, V4R and V8.

From each lead, and regardless of the specific different ways in which different pieces of conventional ECG-collection equipment may perform, what is fed into the system is lead data from these eight leads which, in the case of each lead, is based upon 500-Hz sampling, 5-microvolts per least significant bit, 16-bit information, with simultaneous (from the different leads) samples spanning a duration preferably of about 10-seconds.

As will become apparent from Data Tables that form parts of the present invention disclosure, the unique algorithmic structure of the present invention examines different R/Q and R/S voltage-amplitude ratios that are associated variously with ECG data derived from leads I (ratio R/Q), AVL (ratio R/Q), AVF (ratio R/Q), V1 (ratio R/3), V2 (ratio R/S), V4 (ratios R/Q, R/S), V5 (ratios R/Q, R/S), V6 (ratios R/Q, R/S), V4R (ratio R/S), V8 (ratio R/Q).

In addition to ECG lead information from the leads, and of the category, mentioned above, also provided as input data for implementation of the invention is certain subject- or patient-specific data, including, for example, age, gender and race.

This "block" of data is fed into the system wherein the very first step that is performed involves the detection of so-called confounders and excluders. Confounders include certain conditions, such as right bundle branch block (RBBB), left anterior fascicular block (LAFB) and left ventricular hypertrophy (LVH). Excluders include

conditions such as the presence of a pacemaker, left bundle branch block (LBBB), Wolff-Parkinson-White syndrome, and others.

The presence of confounders and/or excluders fundamentally determines how and to some extent whether data interpretation and analysis proceeds, and the algorithms proposed by the present invention are designed to be capable of dealing with certain patterns of such first-level detected conditions present in the ECG input data.

Following determination of the presence and/or absence of confounders and/or excluders, and assuming that interpretation and analysis is determined to be doable by the system which employs the algorithms of the present invention, the ECG (and accompanying other personal data is subjected to measurements which look at various qualities of the ECG waveforms per se, and also including a look, where appropriate, and in accordance with a feature of the present algorithms, at certain vector ECG information. Based upon these selected measurements, analysis proceeds to determine, first of all, whether or not an old MI is present, and, following that, and if such a condition is detected, to perform an analysis regarding size and location.

### Description of the Drawings

Fig. 1 in the accompanying single sheet of block-diagram sketches illustrates the overall system just generally discussed. The phrase "Stage I" is employed in this figure to characterize the operation of the blocks shown there which relate to the detection of confounders and excluders, and to the obtaining of measurements from input ECG data. The phrase "Stage II" is employed in Fig. 1 to characterize that region pictured therein which relates specifically to the algorithms constructed and employed according to the

present invention. Two phases of algorithmic behavior are illustrated here, the first of which involves the process of detecting, in a “yes/no” sense, the presence or absence of an old MI condition. The second phase involves interpretation to give an indication of size and location of such a condition if one is found to be present.

5 Figs. 2 and 3 in the sketches collectively further detail the “Stage II” portion of Fig. 1, with Fig. 2 further detailing the algorithmic approach proposed herein for the detection of old MI, and with Fig. 3 further detailing the algorithmic approach employed for the interpretation of size and location of any detected old MI.

#### Detailed Description, and Best Mode for Carrying Out, the Invention

The enclosed ten Data Tables (Data Tables I-X, inclusive) generally illustrate the architectures of the algorithms of the present invention, and how the input data is handled by these algorithms to effect MI detection, sizing and location.

Table I generally relates to a situation involving ECG data received from a subject  
15 who does not have any confounding or excluding condition. Table II can be read as being an augmentation to Table I which is relevant to such a subject and under circumstances where a 15-lead input ECG protocol is employed. Table III is similar to Table I, except that it specifically relates to a subject with a right bundle branch block (RBBB) confounding condition. Table IV is also similar to Table I, except that it relates  
20 to another type of confounding condition, and namely, a left anterior fascicular block (LAFB) condition. Table V is also similar to Table I, except that here this table relates to the confounding condition known as left ventricular hypertrophy (LVH). Tables VI-IX,

inclusive, simply show different ways of representing various elements found in Tables I-V, inclusive. Table X generally describes algorithmic utilization of data in various ones of the tables previously mentioned for the purpose of applying inferences to make assessments regarding MI sizing and locating. Inferences which are relevant to this determination are discussed in U.S. Patent No. 6,230,048 issued May 8, 2001 entitled “Pictorial-Display Electrocardiographic Interpretation System and Method”, and the entire content of that patent is hereby incorporated herein by reference for the purpose of elaborating the utilization of inferences.

Describing a typical interpretation event utilizing the algorithms of the present invention, with input ECG and personal information fed into the system, and after the presence of any confounders or excluders has been made, and assuming that interpretation is to go forward, what next occurs is the selection of an appropriate MI “detection” table based upon what has been found in the preliminary-analysis (look) at the input data. If that preliminary look describes a patient who has neither a confounding nor an excluding condition, then, a table very much like that presented in Data Table I is selected for the purpose of detection, and modifications are made in parameters seen in PANEL A in this Table in accordance with specific information about the subject involved, as such is set forth in the comments that appear in text below the table. For example, certain modifications will be made in the PANEL A measurement criteria depending upon whether the subject is male or female, Caucasian, black, etc. and also based upon age. The criteria specifically presented in PANEL A is based upon one particular kind of subject, (Caucasian male age 50, for example,) so modifications will

need to be made for most subjects. The algorithm involved here thus performs these virtual modifications of criteria, and then reads the measurement data which has been developed previously for the purpose of making a determination about whether there is or is not an old MI present.

5           In evaluating ECG data from each of the several leads identified in Table I, the vertical list of values, associations and ratios to be assessed in relation to that lead (seen as a list in the table) take the form of a list which includes one or more of (a) non-hierarchical, (b) hierarchical, and (c) a blend of these two, categories of constituents. The algorithm essentially “goes down” that list to find “confirmations” of categories of constituents, assigning a predetermined weighted assessment value to each confirmed constituent up to but not beyond the Lead Maximum Point count (column 3 in PANEL A) permitted according to the algorithm.

Those skilled in the art looking at the algorithmic listing of the per-lead elements, constituents, ratios, relationships, etc. presented in the Data Tables, along with the  
15           weighted assessment values, and the maximum permitted point counts set forth, will readily understand the logic of the hierarchies presented in the tables. The weighted assessment value assignation is done according to the two columns of numbers appearing along the right side of PANEL A in Data Table I. These assessments numbers present are employed for the purpose of declaring the presence or absence of an MI.

20           Such a “yes/no” declaration, if “no” ends the process and if “yes” effectively hands off the interpretation task to the second phase of Stage II algorithmic performance wherein size and location are assessed. Algorithmic assessment of size and location

follows a pattern which is somewhat like the pattern followed by algorithmic detection of MI presence. What first occurs is the selection of an appropriate detection table, based upon subject-non ECG data, and upon the determined presence of confounding, etc. conditions. This table is, as was done earlier, modified where necessary in order to change specific criteria as such had been deemed necessary to tailor the application of the table to the particular subject. When this is done, then under algorithmic control, the input lead data are again read (hierarchically to obtain value-related confirmations) for the purpose now of creating a pattern of twelve different weighted score numbers relating to the twelve recognized segments of the Ideker quadrants of the heart (see the twelve blank rectangles at the lower-right corner of PANEL B in Data Table I, for example).

With these numbers developed, the same are read in accordance with a pre-determined pattern of knowledge-based inferences, such as those described in the prior-filed patent application mentioned above herein, and the overall system, under algorithmic control, outputs an interpretation output signal which contains information that states, for example, that an old MI has indeed been found, and appears to be located at a particular region in the heart, with a certain size.

Thus, the algorithmic approach described herein is capable of taking into account various specialized input conditions, such as the confounding conditions mentioned, specifically takes into account certain pieces of personal data such as race, gender and age, and utilizes separate collections of specially selected criteria for the purpose of detecting, on the one hand, the presence or absence of an MI, and on the other hand, and thereafter, for determining the size and duration of a detected MI. Input data which is

looked at according to the practice of the present algorithms includes not only timing and amplitude information, for example, of ECG waves, but also vector information relative to ECG-derived information. The algorithms specifically implement analyses based upon combined features of ECG waveforms, such as certain ratios between R and Q and R and S waveform constituents, for example, as a refined tool for assessing MI presence, size and location. The use of differentiated criteria for assessing, from input data, the presence or absence of old MI, and then the size and location of a detected MI, the utilization, where appropriate, of selected vector data, and the combining of ECG wave characteristics as an integral algorithmic behavior, produces an interpretation analysis of great sophistication.

While the invention has been disclosed in a particular setting, and in particular forms herein, the specific embodiments disclosed, illustrated and described herein are not to be considered in a limiting sense. Numerous variations, some of which have been discussed, are possible. Applicants regard the subject matter of their invention to include all novel and non-obvious combinations and subcombinations of the various elements, features, functions and/or properties disclosed herein. No single feature, function, element or property of the disclosed embodiments is essential. The following claims define certain combinations and subcombinations which are regarded as useful, novel and non-obvious. Other such combinations and subcombinations of features, functions, elements and/or properties may be claimed through amendment of the present claims or through presentation of new claims in this or in a related application. Such amended and/or new claims, whether they are broader, narrower or equal in scope to the originally



presented claims, are also regarded as included within the subject matter of applicants' invention.

PANEL A				PANEL B											
ECG POINTS (3% LV each)				% INFARCT IN 12 LV SEGS											
Lead	Criteria	Pts a crit	Lead b Max Pt	LAD			RCA			LCX					
				Ant-sept	sup	inf	7	8	9	10	11	12			
I	Sup-api Q>=30ms R/Q<=1 R<=0.2mV	1 1 1	2	1	1					1					
II	Inf-api Q>=40ms Q>=30ms	2 1	2				1	2	2			1			
AVL	Sup Q>=30ms R/Q<=1	1 1	2		2	1		1	1			1			
AVF	Inf Q>=50ms Q>=40ms Q>=30ms R/Q<=1 R/Q<=2	3 2 1 2 1	5				3	2	2		1	1			
V1	Ant Any	1	2	1	2										
	Post R/S>=1	1								1	2				
	R>=50ms	2	4				1	1		2	1	1			
	R>=40ms	1					1			1	1				
	Q&S<=0.3mV	1					1			1	1				
V2	Ant Any Q	1													
	R<=10ms	1	1	2	1										
	R<=0.1mV	1													
	Post R/S>=1.5	1						1		1	1				
	R>=80ms	2	4				1	1		1	2	1			
	R>=50ms	1					1			1	1				
	Q&S<=0.4mV	1									1	2			
V3	Ant Any Q	1													
	R<=20ms	1	1	2	1										
	R<=0.2mV	1													
	RV3<=RV1	1													
V4	Ant- Q>=20ms	1		1	1	1									
	apical R/Q<=0.25	2		3	2	1									
	R/S<=0.25	2													
	R/Q<=0.5	1	3												
	R/S<=0.5	1		1	1	1									
	R<=0.6mV	1													
V5	Apical Q>=30ms	1		1	1	1									
	R/Q<=0.5	2		1	1	2	2								
	R/S<=0.5	2													
	R/Q<=1	1	3												
	R/S<=1	1		1	1	1									
	R<=0.6mV	1													
V6	Post- Q>=30ms	1			1	1		1							
	apical R/Q<=1	2			1	2		3							
	R/S<=1	2													
	R/Q<=2	1	3												
	R/S<=2	1				1		2							
	R<=0.6mV	1													
TOTALS	Points->														
			%LV>												

DATA TABLE I

If > 1 criteria in bracket met, select 1 with most points

If > 1 criteria in bracket has same point, score only once

Age normalize amplitude criteria to age 50, increasing them by

1%/yr for ages 20-49 and decreasing them 1%/yr for >50 yrs.

For Females further decrease all amplitude criteria by 20% → 20%  
and decrease all duration criteria by 10%

PANEL A				PANEL B											
Lead	Criteria	Pts ea crit	Lead Max Pt	L A D			RCA			LCX					
				Ant-sept,sup			Inf			Post-lat					
V8R Post	Q>=70ms	2		<del>0 1 2 3 4 5 6 7 8 9</del>			<del>0 1 2 3 4 5 6 7 8 9</del>			<del>0 1 2 3 4 5 6 7 8 9</del>			<del>0 1 2 3 4 5 6 7 8 9</del>		
	Q>=60ms	1		0 1 2 3 4 5 6 7 8			0 1 2 3 4 5 6 7 8			9 2 4			1 2		
V4R Ant	any Q	1	1	1 2						2 3 1					
Post	R>=36ms	2								1 2					
<del>del</del>	<del>R/S&gt;=4</del>	3	4							2 4 3					
	R/S>=2	2								1 3 2					
	R/S>=1	1								1 2					
V8 Post	Q>=46ms	2								3 3					
	Q>=36ms	1								2 1					
	R/Q>=2	2								1 3 2					
	R/Q>=4	1								2 1					
TOTALS	Points->														
			%LVI>												

DATA TABLE II

DATE: 11/15/01

PANEL A				PANEL B											
ECG POINTS (3% LV each)				% INFARCT IN 12 LV SEGS											
With RBBB				L A D						RCA		LCX			
Lead	Criteria	Pts ea crit	Lead Max Pt	Ant-sept-sup						Inf		Post-lat			
				1	2	3	4	5	6	7	8	9	10	11	12
I Sup-api	Q>=30ms	1					1	1					1		
	R/Q<=1	1	2				2	1							
	R<=0.2mV	1													
II Inf-api	Q>=40ms	2	2							1	2	2		1	
	Q>=30ms	1								1	1			1	
AVL Sup	Q>=30ms	1	2				2	1							
	R/Q<=1	1					1	2							
AVF Inf	Q>=50ms	3								3	2	2		1	1
	Q>=40ms	2								2	2	2			
	Q>=30ms	1	5							2	1				
	R/Q<=1	2								2	3			1	
	R/Q<=2	1								1	2				
V1 Ant	Any Q	1	2		1	2									
	Post R/S>=1	1										1	2		
	R>=50ms	2	4							1	1	2	1	1	
	R>=40ms	1								1		1	1		
	Q&S<=0.3mV	1								1		1	1		
V2 Ant	Any Q	1													
	R<=10ms	1	1		2	1									
	R<=0.1mV	1													
	Post R/S>=1.5	1								1		1	1		
	R>=60ms	2	4							1	1	1	2	1	
	R>=50ms	1								1		1	1		
	Q&S<=0.4mV	1										1	2		
V3 Ant	Any Q	1													
	R<=20ms	1	1		2	1									
	R<=0.2mV	1													
	RV3<=RV1	1													
V4 Ant-	Q>=20ms	1			1	1	1								
apical	R/Q<=0.25	2			3	2	1								
	R/S<=0.25	2													
	R/Q<=0.5	1	3		1	1	1								
	R/S<=0.5	1													
	R<=0.6mV	1													
V5 Apical	Q>=30ms	1			1	1	1								
	R/Q<=0.5	2			1	1	2	2							
	R/S<=0.5	2													
	R/Q<=1	1	3		1		1	1							
	R/S<=1	1													
	R<=0.6mV	1								1		2			
V6 Post-	Q>=30ms	1				1		1		1		1			
apical	R/Q<=1	2				1		2				3			
	R/S<=1	2													
	R/Q<=2	1	3												
	R/S<=2	1								1		2			
	R<=0.6mV	1													
TOTALS Points->															
				%LVI>											

DATA TABLE III

If > 1 criteria in bracket met, select 1 with most points  
 If > 1 criteria in bracket has same point, score only once  
 Are normalize amplitude criteria to are 50 increasing them by

PANEL A				PANEL B											
ECG POINTS (8% LV each)				% INFARCT IN 12 LV SEGS											
With LAFB		Pts	Lead	I A D						RCA			L C X		
Lead	Criteria	ea	Max	Ant-sept,-sup						Inf			Post-lat		
		crit	Pt	1	2	3	4	5	6	7	8	9	10	11	12
I Sup-api	Q>=30ms	1						1	1				1		
	R/Q<=1	1	2					2	1						
	R<=0.2mV	1													
II Inf-api	Q>=40ms	2	2							1	2	2		1	
	Q>=30ms	1								1	1			1	
AVL Sup	Q>=40ms	1	2					2	1						
	R/Q<=1	1						1	2						
AVF Inf	Q>=50ms	3								3	2	2		1	1
	Q>=40ms	2								2	2	2			
	Q>=30ms	1	5							2	1				
	R/Q<=1	2								2	3			1	
	R/Q<=2	1								1	2				
V1 Ant	Any Q	1	2	1	2										
	Post R/S>=1	1											1	2	
	R>=50ms	2	4							1	1		2	1	1
	R>=40ms	1								1			1	1	
	Q&S<=0.3mV	1								1			1	1	
V2 Ant	Any Q	1													
	R<=10ms	1	1	2	1										
	R<=0.1mV	1													
	Post R/S>=1.5	1									1		1	1	
	R>=60ms	2	4							1	1		1	2	1
	R>=50ms	1								1			1	1	
	Q&S<=0.4mV	1												1	2
V3 Ant	Any Q	1													
	R<=20ms	1	1	2	1										
	R<=0.2mV	1													
	RV3<=RV1	1													
V4 Ant-	Q>=20ms	1		1	1	1									
apical	R/Q<=0.25	2		3	2	1									
	R/S<=0.25	2													
	R/Q<=0.5	1	3												
	R/S<=0.5	1		1	1	1									
	R<=0.6mV	1													
V5 Apicl	Q>=30ms	1		1	1	1									
	R/Q<=0.5	2		1	1	2	2								
	R/S<=0.5	2													
	R/Q<=1	1	3												
	R/S<=1	1		1		1	1								
	R<=0.6mV	1													
V6 Post-	Q>=30ms	1				1		1		1			1		
apical	R/Q<=1	2				1		2					3		
	R/S<=1	2													
	R/Q<=2	1	3												
	R/S<=2	1								1			2		
	R<=0.6mV	1													
TOTALS Points->															
				%LVI>											

DATA TABLE IV

PANEL A				PANEL B											
ECG POINTS (3% LV each)				% INFARCT IN 12 LV SEGS											
With LVH ± LAFB		Pts ea	Lead Max	L A D			RCA			L C X					
Lead	Critera	crit	Pt	1	2	3	4	5	6	7	8	9	10	11	12
I Sup-apl	Q>=30ms	1					1	1					1		
	R/Q<=1	1	2				2	1							
	R<=0.2mV	1													
II Inf-apl	Q>=50ms	2	2							1	2	2		1	
	* Q>=40ms	1								1	1			1	
AVL Sup	Q>=40ms	1	2				2	1							
	R/Q<=1	1					1	2							
AVF Inf	Q>=60ms	3								3	2	2		1	1
	* Q>=50ms	2								2	2	2			
	* Q>=40ms	1	5							2	1				
	R/Q<=1	2								2	3			1	
	R/Q<=2	1								1	2				
V1 Ant	* Any QR	1	2		1	2									
	Post R/S>=1	1											1	2	
	* R>=56ms	2	4							1	1		2	1	1
	* R>=48ms	1								1			1	1	
	Q&S<=0.3mV	1								1			1	1	
V2 Ant	* Any QR	1	1		2	1									
	RV2<RV1	1													
	Post R/S>=1.5	1								1			1	1	
	* R>=66ms	2	4							1	1		1	2	1
	* R>=58ms	1								1			1	1	
	Q&S<=0.4mV	1											1	2	
V3 Ant	* Any QR	1													
	* R<=10ms	1	1		2	1									
	* R<=0.1mV	1													
	RV3<RV1	1													
V4 Ant-	Q>=20ms	1			1	1	1								
apical	R/Q<=0.25	2			3	2	1								
	R/S<=0.25	2													
	R/Q<=0.5	1	3												
	R/S<=0.5	1			1	1	1								
	R<=0.6mV	1													
V5 Apical	Q>=30ms	1			1	1	1								
	R/Q<=0.5	2			1	1	2	2							
	R/S<=0.5	2													
	R/Q<=1	1	3												
	R/S<=1	1			1		1	1							
	R<=0.6mV	1													
V6 Post-	Q>=30ms	1					1		1				1		
apical	R/Q<=1	2					1		2				3		
	R/S<=1	2													
	R/Q<=2	1	3												
	R/S<=2	1							1				2		
	R<=0.6mV	1													
TOTALS	Points->														
			%LVI>												

DATA TABLE V

Detection Criterial Threshold:

Criteria Thresholds (in mV and ms)	Threshold	RBBB	LAFB	RVH	LVH	Points	Location	Notes
I Q Dur >=	34					2	A	1
II R/Q <=	3					2	A	
III Q Dur >= OR	32				32	1	I	
II R/Q <= I	4					1	I	
aVL Q >= OR	36				36	1	A	
aVL Q Dur w/ neg T aVL T >= I	32				32	1	A	
aVF Q Dur >= OR	34				34	2	I	2
aVF Q Dur w/ neg aVF T >= I	24				24	-		3
aVF R/Q <=	1.8					1	I	
V1 Q Dur >=	0					1	A	
V1 R/S >= OR	1.6	X		X		1	P	
V1 R Dur >= I	50	X		X		1	P	
V1 Q & S <=	200	X		X		1	P	
V2 Ant Q Dur >=	0				QandR	1	A	4
V2 Post R/S >=	5	X		X		1	P	
V2 Post R Dur >=	58	X		X		1	P	
V3 Q Dur >=	24					1	A	
V4 Q Dur >=	36					1	A	
V4 R/Q <= OR	3					1	A	
V4 R/S <= OR	0.3					1	A	
V4 R Amp <= I	400				600	1	A	
V5 Q Dur >=	32					2	A	
V5 R/Q <= OR	5					2	A	
V5 R/S <= OR	0.7				1.5	1	A	
V5 R Amp <= I	400				500	1	A	
V6 Q Dur >=	32					1	P	
V6 R/S <=	2				1.5	1	P	
Points for 3 Inf neg T's OR						2	I	
Points for 2 Inf neg T's						1	I	
Points for 2 Ant neg T's						1	A	
Points for 1 aVL neg T's						1	A	
Points for V2T-V6T >=	600				X	1	P	
V2R dur <= AND	20				X	-	-	
V2R+V3R dur <= I	40				X	1	A	5
Anterior Duration <= AND	18					1	A	6
Anterior Distance <= AND	400					-	-	
Max Posterior Amplitude >= I	50					-	-	
Superior Distance >= AND	300					1	I	7
Max Superior Amplitude >= I	100					-	-	
Anterior/Posterior Ratio >= AND	2	X		X		1	P	8
Max Anterior Amplitude >= I	500					-	-	

NOTES:

1. aVL Q Threshold changed based on presence on negative T in aVL AND I (Tamp <= T amp Threshold).
2. aVF Q scores 2 points if II Q >= 26mS, otherwise aVF Q scores 1 point.
3. aVF Q Threshold changed based on presence on negative T in aVF (aVF T amp <= T amp Threshold).
4. With LVH present, a Q followed by an R must be present to score points (Q only does not score).
5. One point for: [V2R <= 20mS] AND [(V2R+V3R) <= 40mS].
6. One point for: [Anterior Duration <= 18] AND [Anterior Distance <= 400]
7. One point for: [Superior Distance >= 300] AND [Max Superior Amp >= 100]
8. One point for: [Max Anterior Amp >= 500] AND [(Max Anterior Amp)/Max Posterior Amp >= 2]
9. An X indicates the criteria is disabled if the given confounder is true.

DATA TABLE VI

BEST AVAILABLE COPY

60 yr. old male

Criteria	Thresholds (in $\mu$ V and ms)	RBBB	LAFB	RVH	LVH
I Q Dur $\geq$	34				
I R Q $\leq$	-1				
I R Amp $\leq$	-1				
I R Q $\leq$	-1				
II Q Dur $\geq$	1000				
II Q Dur $\geq$	32				32
aVL Q $\geq$	34				34
aVL Q Qual Dur $\geq$	30				30
aVL R Q $\leq$	-1				
aVF Q Dur $\geq$	1000				
aVF Q Dur $\geq$	1000				
aVF Q Dur $\geq$	34				34
aVF Q Qual Dur $\geq$	24				24
aVF R Q $\leq$	-1				
aVF R Q $\leq$	1.8				
V1 Q Dur $\geq$	0				
V1 R/S $\geq$	1.6	X		X	
V1 R Dur $\geq$	1000				
V1 R Dur $\geq$	54	X		X	
V1 Q & S $\leq$	200	X		X	
V2 Ant Q Dur $\geq$	0				QandR
V2 Ant R Dur $\leq$	-1				X
V2 Ant R Amp $\leq$	-1				X
V2 Post R/S $\geq$	5	X		X	
V2 Post R Dur $\geq$	1000				
V2 Post R Dur $\geq$	58	X		X	
V2 Q & S $\leq$	-1	X		X	
V3 Q Dur $\geq$	1000				
V3 R Dur $\leq$	-1				
V3 R Amp $\leq$	-1				
V3 Q Dur $\geq$	24				
V3 R Dur $\leq$	-1				
V3 R Amp $\leq$	-1				
V4 Q Dur $\geq$	1000				
V4 R Q $\leq$	-1				
V4 R/S $\leq$	-1				
V4 R Q $\leq$	3				
V4 R/S $\leq$	0.3				
V4 R Amp $\leq$	-400				600
V5 Q Dur $\geq$	34				
V5 R Q $\leq$	-1				
V5 R/S $\leq$	-1				
V5 R Q $\leq$	5				
V5 R/S $\leq$	0.7				1.5
V5 R Amp $\leq$	370				500
V6 Q Dur $\geq$	34				
V6 R Q $\leq$	-1				
V6 R/S $\leq$	-1				
V6 R Q $\leq$	-1				
V6 R/S $\leq$	1.8				1.5
V6 R Amp $\leq$	-1				-1
T amp $\leq$	-75				
Points for 3 Int neg Ts	1				
Points for 2 Int neg Ts	1				
Points for 2 Ant neg Ts	1				
V2 R dur $\leq$	20				
V2 R + V3 R dur $\leq$	40				X
Anterior Duration $\leq$ (Ant)	15				
Superior Distance $\geq$	450				

DATA TABLE VII

BEST AVAILABLE COPY



ECG Points 3% LV each										% LV Infarct In 12 Segments																
Lead	Criteria	Nominal Threshold	Confounder Adjustments				Amp or Dur Adjustment	Notes	Pts each	Lead Max Points	LAD						RCA			LCX						
			RBBB	RVH	LAFB	LVH					Ant-sept, sup	1	2	3	4	5	6	7	8	9	10	11	12			
Lead I Sup-apl	Q dur >=	34mS	-	-	-	-	-	Yes	1	2	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1
	{ I/R/Q <= OR R <= }	0.15mV	-	-	-	-	-	Yes	1	1	2	1	2	1	2	1	2	1	2	1	2	1	2	1	2	1
Lead II Inf-apl	Q dur >= OR	40mS	-	-	-	50mS	-	Yes	2	3	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2
	Q dur >= OR	32mS	-	-	-	40mS	-	Yes	1	1	2	1	2	1	2	1	2	1	2	1	2	1	2	1	2	
Lead aVL Sup	Q dur >= }	-	-	-	-	32mS	-	No	1	1	2	1	2	1	2	1	2	1	2	1	2	1	2	1	2	
	Ramp/Qamp <=	4	-	-	-	-	-	-	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
Lead aVF Sup	Q dur >= OR	32mS	-	-	40mS	40mS	-	Yes	1	2	1	2	1	2	1	2	1	2	1	2	1	2	1	2	1	
	Q dur >= OR	-	-	-	36mS	36mS	-	No	1	1	1	2	1	2	1	2	1	2	1	2	1	2	1	2	1	
Lead aVF Inf-apl	Qdur >= xx w/ neg I&aVL T }	32mS	-	-	32mS	32mS	-	No	1	1	1	2	1	2	1	2	1	2	1	2	1	2	1	2	1	
	Ramp/Qamp <=	1	-	-	-	-	-	-	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
Prominent Initial Superior Forces Inf	{ Q >= OR	50mS	-	-	-	60mS	-	Yes	3	5	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	
	Q >= OR	42mS	-	-	-	50mS	-	Yes	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	
Lead V1 Ant	Q >= OR	34mS	-	-	-	40mS	-	Yes	1	1	2	1	2	1	2	1	2	1	2	1	2	1	2	1	2	
	Q >= OR	-	-	-	-	34mS	-	No	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
Post 12L scoring	Qdur >= xx w/ neg aVF T }	24mS	-	-	-	24mS	-	No	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
	{ Ramp/Qamp <= OR	1	-	-	-	-	-	-	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	
Post 15L scoring	Ramp/Qamp <= 1 }	2	-	-	-	-	-	-	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
	[ Suprior Distance >= AND Maximum Superior Amplitude >= ]	300 100	-	-	-	-	-	-	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
Lead V1 Post	Q dur >= (any Q)	0mS	-	-	-	X	-	-	2	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
	Q dur >= AND R dur >= (any QR)	X	-	-	-	0mS	-	-	2	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
Post 12L scoring	Ramp/Samp >=	1.3	X	X	-	-	-	-	1	2	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
	{ (Qamp AND Samp) <= OR (Qamp AND Samp) <= }	0.15mV 0.20mV	X	X	-	-	-	Yes	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
Post 15L scoring	{ R dur >= OR	56mS	X	X	-	-	-	Yes	3	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	
	R dur >= }	48mS	X	X	-	-	-	Yes	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
Lead V2 Ant	{ R dur >= OR	56mS	X	X	-	-	-	Yes	3	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
	R dur >= }	50mS	X	X	-	-	-	No	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
Post 12L scoring	{ Q dur >= (any Q) OR	0mS	-	-	-	X	-	-	2	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
	R dur <=	10mS	-	-	-	X	-	Yes	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
Post 15L scoring	R amp <= }	0.04mV	-	-	-	X	-	Yes	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
	Q dur >= AND R dur >= (any QR)	X	-	-	-	0mS	-	-	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
Prominent	Ramp/Samp >=	3	X	X	-	-	-	-	1	2	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
	{ (Qamp AND Samp) <=	0.30mV	X	X	-	-	-	Yes	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
Post 12L scoring	{ R dur >= OR	64mS	X	X	-	-	-	Yes	3	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	
	R dur >= }	56mS	X	X	-	-	-	Yes	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
Prominent	{ R dur >= OR	64mS	X	X	-	-	-	Yes	3	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	
	R dur >= }	58mS	X	X	-	-	-	No	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	



## Scoring Table for Sizing and Locating

### How to Read the Table:

1. A 'Yes' in the 'Amp or Dur Adjustments' column indicates the Nominal Threshold is adjusted for race, age, and gender (see adjustment instructions below).
2. Change threshold if a Confounder is detected and a new threshold value is indicated in the Confounder Column.
3. An 'X' indicates the criteria is ignored if the Confounder is True. Example: V1 R/S is not scored if RBBB is detected.
4. A '-' indicates no change in criteria if the Confounder is True.
5. The {} symbol indicates an OR function. Once a criteria in an OR function is met, score the appropriate points, then skip the subsequent tests in the OR brackets.
6. The [] symbol indicates the AND function. All criteria inside the AND function must be met to score points.

### Adjustments for Race, Age, and Gender:

Some amplitude and duration criteria thresholds are adjusted for Race, Age and Gender. No criteria adjustments are made to ratio criteria (Ramp/Qamp or Ramp/Samp). Refer to the column labeled "Amp or Dur Adjustment" to determine whether an individual criteria should undergo amplitude or duration adjustments.

Amplitude Adjust:	Age:	Normalize to 50 years. Threshold = Nominal Threshold * (1 + (50-patient age)/100)
	Gender:	Male, No adjustment;
	Race:	Female: Reduce Threshold by 20% (multiply threshold by 0.8)
		Black: Increase threshold by 120%
		All others: No adjustments
Duration Adjust:	Gender:	Male, No adjustment;
		Female: Reduce Threshold 10% (multiply threshold by 0.9)

### Notes: (Refer to Table, Column heading "Notes")

1. Score points for "Prominent Initial Superior Forces" only when none of the following Criteria are met:  
II Q >=; aVF Q >=
2. Score one point for any Q unless LVH is present. If LVH detected, then 1 point scored for a Q followed by an R (Q or R only does not score)
3. Score 12 lead criteria for 12 lead ECG; Score 15 lead criteria for 15 lead ECG
4. Score points for "Prominent Anterior Forces" only when none of the following Criteria are met:  
V1 R/S >=; V1 R dur >=; V1 Q&S <=; V2 R/S >=; V2 R dur >=; V2 Q&S <=; CZ Q dur >=; V8 R amp <=
5. Score points for "V2 Tamp - V6 Tamp >=" only when none of the following Criteria are met:  
V1 R/S >=; V1 R dur >=; V1 Q&S <=; V2 R/S >=; V2 R dur >=; V2 Q&S <=; CZ Q dur >=; V8 R amp <=; Prominent Anterior Forces
6. Score points for "Minimal Initial Anterior Forces" only when none of the following Criteria are met:  
V2 Any Q; V2 R dur <=; V2 R amp <=; V3 R amp <=
7. Score points for "V2R dur + V3Rdur >=40ms" only when none of the following Criteria are met:  
V2 Any Q; V2 R dur <=; V2 R amp <=; V3 R amp <=; Minimal Initial Anterior Forces

DATA TABLE X